

Computational Risk Assessment of Ventricular Tachycardia based on Myocardial Scarring Characterization

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Introduction: Myocardial scarring is typically modelled as non-conductive tissue. We demonstrate employing electrophysiology simulations that detailed micro- and macroscopic modelling of non-ischemic (*Test 1*) and ischemic (*Test 2*) alterations enables patient-specific arrhythmic risk assessment.

Methods: We employed the Ten Tusscher-Panfilov ionic model for cellular behaviour and the monodomain model for macroscopic propagation.

In *Test 1*, Magnetic Resonance Imaging (MRI) and electro-anatomical mapping (S. M. del Carmine Hospital) were used for ventricular and non-ischemic fibrosis segmentation and for electrical conductivity calibration. In this context, to define suitable ionic models for non-ischemic cardiomyopathies, an optimization framework was developed in collaboration with Inria to calibrate ionic parameters against available optical mapping data.

In *Test 2*, we exploited MRI (Centro Cardiologico Monzino) for the segmentation of left ventricles and ischemic scars, modelling the latter with conductive channels generated via an open-source Perlin noise algorithm.

Results: Arrhythmogenic substrates were evaluated through ectopic simulations performed using LifeX (Finite Elements library developed at MOX and LaBS, Politecnico di Milano) at fibrosis/scar borders.

In *Test 1*, the optimization framework successfully fitted the simulated action potential to optical data, enabling the replication of experimental traces (Fig.1, left). Moreover, simulations correctly identified the clinical status of three patients: two were classified as arrhythmic due to high reentry incidence (6/10 arrhythmic ectopic sites), one was non-arrhythmic (3/10) (Fig.1, left).

In *Test 2*, the inclusion of conductive channels within the scar, rather than treating it as a non-conductive obstacle, promoted the formation of reentry circuits (Fig.1, right), matching clinical follow-up data. Conversely, modelling pathological regions as non-conductive oversimplifies the complexity of the substrate, leading to underestimated risks.

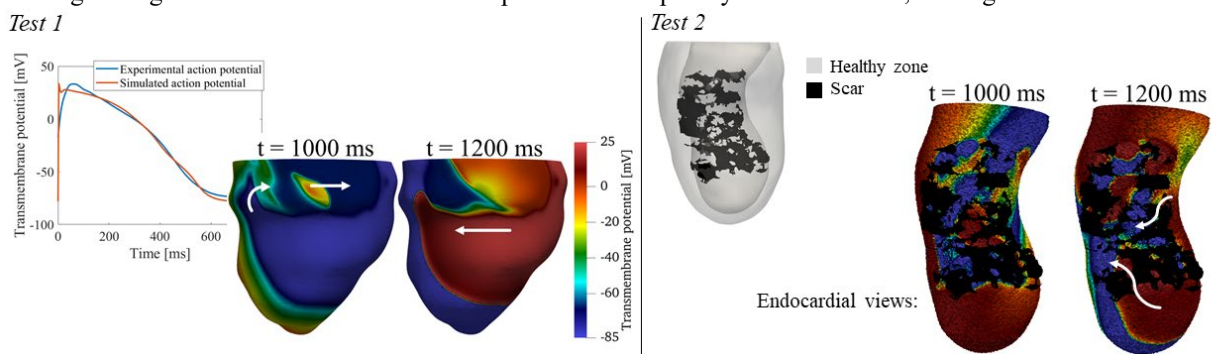


Fig.1. Left: *Test 1*. Output from the calibration process and evolution of a reentry; the arrows indicate the direction of the wavefront. Right: *Test 2*. Representation of conductive channels and visualization of the propagation pattern of a reentry.

Conclusion: These findings identify computational electrophysiology as a powerful non-invasive tool for patient-specific risk stratification. Moving beyond the non-conductive approximation by linking arrhythmogenic risk to substrate heterogeneity is essential to refine clinical treatment criteria.

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