Choosing Electrogram Features for Predicting Catheter Ablation Outcomes in Persistent Atrial Fibrillation

Noor Qaqos¹, Fernando S Schlindwein^{1,3}, G André Ng^{2,3}, Xin Li^{1,3}

¹School of Engineering, University of Leicester, Leicester, UK ²Department of Cardiovascular Sciences, University of Leicester, Leicester, UK ³National Institute for Health Research Leicester Cardiovascular Biomedical Research Centre, UK

Abstract

The rate of successful outcomes of catheter ablation to treat persistent atrial fibrillation (persAF) using individual features including dominant frequency (DF), complex fractionated atrial fibrillation (CFAE), and rotors have been disappointing. We aim to identify the most important electrogram (EGM) features for successful ablations using a Random Forest (RF) classifier. A total of 3206 EGMs were collected using non-contact mapping catheter from 10 patients. 1490 EGMs were labelled as positive responses to ablation and 1716 EGMs as negative. Features were extracted from the three EGM signal domains (spectral, temporal and statistical) using time series feature extraction library in python. Five-fold cross validation (CV) was used for training and testing the classifier. A CV accuracy of 80.54% and F1 score of 78.23% were achieved for classifying the responses of EGMs to catheter ablation, with a sensitivity of 75.2% and specificity of 85.14%. RF showed potential for predicting the responses of EGMs to catheter ablation and finding the most important features. These features are the power spectral density (PSD) at 10Hz, the mean and the mean voltage of differences for spectral, statistical and temporal domains, respectively. This will further inform the further development of key features of EGMs for guiding catheter ablation in persAF.

1. Introduction

In clinical practice, atrial fibrillation (AF) is the most common sustainable arrhythmia, and uncoordinated activation of the atria is the main cause of such type of arrythmia. AF is relevant with the incidence of stroke, heart failure and the cardiac death in adults [1, 2], as the AF condition leads to blood clots in the atria due to the lack of effective atrial contraction in AF patients. AF therapy aims to restore the sinus rhythm. Medication has been used to regulate the heartbeat, but some AF patients continue to sustain AF in spite of medication treatment[3]. Catheter ablation is commonly employed to treat paroxysmal AF, but it is less effective for persistent AF (persAF), due to different mechanisms that initiate and maintain persAF [4]. Features using traditional methods such as DF [5], CFAE [6] and rotors [7] have not shown be sufficient to guide persAF ablation. Therefore, researchers have been searching for other features in EGMs to guide AF ablations. Features of EGMs represented by the power spectrum play an important role in treating the AF for the accepted frequency in human which is in the range between 3-15 Hz [5]. Voltage of the signals also has an impact to discriminate the regions that harbour the AF drivers. The low voltage regions in the atria are more dominant to harbour the AF [8-10]. Therefore, EGM features that are mentioned above might be good sites to terminate and enhance catheter ablation to treat the persAF. Machine learning techniques have been widely used to detect AF using ECG signals, but the utility of these techniques in raw EGMs classification based on positive or negative responses to catheter ablation has been explored for few works.

2. Materials and Methods

2.1. Dataset

The dataset was collected from 10 persAF patients undergoing left atrium (LA) catheter ablation for the first time. The high dominant frequency (HDF) regions were identified as described before [11]. The dataset was collected using non-contact basket mapping catheter using Ensite array, St. Jude Medical, 2048 nodes. EGMs were exported to the MATLAB platform and ablation was guided by DF. After the ablation process 4 out of 10 patients had AF termination (1 sinus rhythm and 3 flutters) before the pulmonary vein isolation (PVI). EGMs of up to 20 seconds were exported from all patients before ablation procedure to train and test the RF classifier.

2.2. Data Labelling

The dataset was labelled based on AF cycle lengths (AFCL) criterion. The AFCL before and after ablation was calculated in a total of 51 locations (3206 EGMs) identified by HDF of 10 patients. Two classes of pre-ablation EGMs were considered as labels: positive and negative responses to catheter ablation. A positive response was identified by AF termination or AFCL increase (\geq 10ms), whereas negative response by AFCL decrease (\leq 10ms) [2] or AFCL unchange. A total of 3206 nodes were classified:1716 as negative and 1490 as positive responses.

2.3. Pre-processing

The 20 seconds of the collected EGMs were sampled at 2034.5Hz and then re-sampled to 512Hz to reduce the memory requirements for storage. QRST subtraction was performed to remove the effect of the far-field from the ventricle [12]. The middle window in Figure 1 shows the QRST subtraction process for EGM signal.

2.4. Feature Extraction

A total of 390 features were extracted from the EGMs using time series feature extraction library (TSFEL) [13]. This library is designed and implemented to be suitable for feature extraction from biomedical signals. The library extracted features from the EGMs in three domains (spectral, temporal and statistical). The extracted features from this library are shown in table 1.

2.5. Feature Selection

Feature selection process was performed to remove the features that are highly correlated and low variance. Pearson's correlation method with a threshold of 75% was used to remove the high correlated features. Low variance features were also removed with threshold of 0, where the EGM feature was removed from the feature set when the feature has exactly the same value for all EGM samples.

2.6. Feature Importance

A total of 32 features were resulted from the feature selection step. RF classifier was used to score of these features and then sequenced them based on their importance in the classification process. Figure 2 shows the features importance based on mean decrease in impurity (MDI) (Gini importance) criterion, which counts the times a feature is used to split a node, weighted by the number of samples it splits.

Table 1.Features extra	cted using TSFEL [13]

SPECTRAL DOMAIN	TEMPORAL	STATISTICAL
	DOMAIN	DOMAIN
 FFT Mean Coefficients 	Absolute energy	• ECDF (#10)
(#256)	 Area Under the 	 ECDF Percentile
 Fundamental Frequency 	Curve	(#2)
 Human Range Energy 	 Autocorrelation 	 ECDF Percentile
• LPCC (#13)	 Centroid 	Count (#2)
 Maximum Frequency 	 Entropy 	 Histogram (#10)
 Maximum Power 	 Negative turning 	 Interquartile
Spectrum	points	Range
 Median Frequency 	 Mean Absolute 	 Kurtosis
 MEL Frequency 	Difference	 Maximum
Cepstral Coefficients	Mean	 Mean
(#12)	differences	 Mean Absolute
 Power Bandwidth 	 Median 	Deviation
 Spectral Centroid 	Absolute	 Median
 Spectral Decrease 	Difference	 Median Absolute
 Spectral Distance 	Median	Deviation
 Spectral Entropy 	Difference	 Minimum
 Spectral Kurtosis 	• Positive turning	 Root Mean Square
 Spectral Positive turning 	points	 Skewness
points	Peak to Peak	 Standard
 Spectral Roll-off 	Distance	Deviation
 Spectral Roll-On 	• Signal Distance	 Variance
 Spectral Skewness 	• Slope	
 Spectral Slope 	• Sum Absolute	
 Spectral Spread 	Difference	
 Spectral Variation 	• Total energy	
 Wavelet Absolute Mean 	Zero Crossing	
(#9)	Rate	
• Wavelet Energy (#9)	 Ineignbornood 	
 Wavelet Entropy 	peaks	
 Wavelet Standard 		
Deviation (#9)		
Wavelet Variance (#9)		
# Spectral	#Temporal	# Statistical
features = 336	features = 18	features = 36
#Total features = 390		



Figure 1. The complete diagram for the proposed method

2.7. **RF Model Training**

RF classifier was implemented using anaconda

environment with python 3.8 for simulation. Five-fold cross validation technique was applied to a total of 3206 EGMs for training and testing the model. The classifier was trained using 80% (2565 EGMs) and tested on 20% (641 EGMs) of the dataset. The 3 most important features were selected to train and test the model, which can speed up the training process and also make them easier to analyse for guiding the ablation procedure. These features represented by FFT mean coefficient at 10Hz (PSD at 10 Hz) as the spectral domain feature, mean voltage of signal as a statistical domain feature and mean voltage of differences as the temporal domain feature. Grid search algorithm was applied to set and optimise the parameters' tunning as below:

- Max_depth = 5, and represents the number of splits for the decision tree in the RF trees is allowed to make. The number from 3-5 is good to prevent the overfitting of the RF classifier.
- N_estimators =10, and represents the number of trees in the forest.
- Criterion='gini', Gini was used as a criterion to evaluate the feature's importance.



Figure 2. Importance of features based on MDI

3. **Results and Discussion**

A RF classifier was used to classify the EGMs based on their positive or negative responses to catheter ablation. A total of 3206 labelled EGMs were used, with 2565 EGMs used as a train set, and 641 as a test set. The trained RF classifier achieved overall accuracy (5-fold-CV accuracy) of 80.54%.

3.1 CM and ROC

The confusion matrix (CM) for the trained RF classifier is shown in Figure 3a. This figure shows the number of true positive and negative responses in comparison with the total number of EGMs responses. It can be seen that the trained classifier achieved an overall accuracy 80.54% using 5-fold CV technique, whereas it performed 75.2%, 85.14% and 78.23% for a sensitivity, specificity and the F1_score, respectively. Receiver operating characteristics (ROC) and the area under the

curve (AUC) for the positive class are shown in Figure 3b. It can be noticed that the AUC for the trained classifier was 0.91.

3.2 Statistical Feature Analysis

The unpaired t-test was used to analyse the 3 most important features. Unpaired t-test using Welch's correction were applied to analyse the binary RF model. Figure 4 shows the mean and the standard deviation for the 3 most important features. The mean of PSD at 10Hz for the positive and negative classes were 0.0018±0.0013 and 0.0015 ± 0.0024 . The mean voltages were 0.011 ± 0.036 and 0.027±0.055, while the mean differences were $-2.2 \times 10^{-6} \pm 5.5 \times 10^{-5}$ and $1.5 \times 10^{-5} \pm 6.8 \times 10^{-5}$, respectively. P-value for the two classes was <0.0001. These results support the recent findings that PSD of EGMs has an impact for successful ablation [5]. In this work, EGM regions that responded positively to catheter ablation have higher PSD at 10Hz, and also atrial regions with low voltage and high frequency are more likely to harbour AF drivers [8, 9]. Low voltage areas in left atrial are the marker for presence of fibrosis areas [10]. Therefore, it is noticed that the features of the positive class were different from those of the negative class. This indicates that atrial regions responsible for AF exhibit distinct characteristics compared to non-AF regions.



Figure 3. CM and ROC for the trained RF classifier



Figure 4. The bar graph of 3 most important features.

4. Model Employment and Limitations

The RF trained model applied to all data points (2048) including the nodes/EGMs that are not ablated for predicting the responses of EGMs to catheter ablation. Figure 5 shows the 3D geometry of 10 patients. The left

atrium of all patients is color-coded by the prediction of RF model, whereas the color-coded dots are the actual ablation responses. The limitation of this work represents by the number of patients. Therefore, more patients with more ablation lesion dataset would assist to enrich the trained classifier with more knowledge for classification of EGMs responses for inter-patients' differences.



Figure 5. The 3D geometry of left atrium of 10 patients

5. Conclusions

This paper aims to identify the most important features associated to the initiation and maintenance of persAF from three EGM signal domains (spectral, temporal and statistical). Twenty seconds of EGM duration were used in the proposed method. Features based on three EGM domains were extracted from each signal. The importance for each feature was calculated based on mean decreased in impurity. The most important features using RF classifier represented by PSD for spectrum frequency 10Hz for spectral domain, mean voltage for the statistical domain and mean voltage of differences for the temporal domain of the signals. These important findings may suggest that targeting the sites with these features might lead to an improvement of the success rate of catheter ablation for treating the persAF. The accuracy of trained RF classifier based on these features was 80.54%.

References

- [1] G. F. Michaud, and W. G. Stevenson, "Atrial fibrillation," N Engl J Med, vol. 384, no. 4, pp. 353-361, Jan 28, 2021.
- [2] T. P. Almeida, X. Li, B. Sidhu, A. S. Bezerra, M. Ehnesh, I. Anton, I. A. Nasser, G. S. Chu, P. J. Stafford, and T. Yoneyama, "Dominant frequency and organization index for substrate identification of persistent atrial fibrillation," *Computing in Cardiology*, vol. 48, pp. 1-4, Jan 10, 2021.
- [3] A. European Heart Rhythm, S. European Association for Cardio-Thoracic, A. J. Camm, P. Kirchhof, G. Y. Lip, U. Schotten, I. Savelieva, S. Ernst, I. C. Van Gelder, N. Al-Attar, G. Hindricks, B. Prendergast, H. Heidbuchel, O. Alfieri, A. Angelini, D. Atar, P. Colonna, R. De Caterina, J. De Sutter, A. Goette, B. Gorenek, M. Heldal, S. H.

Hohloser, P. Kolh, J. Y. Le Heuzey, P. Ponikowski, and F. H. Rutten, "Guidelines for the management of atrial fibrillation: the task force for the management of atrial fibrillation of the european society of cardiology (ESC)," *Eur Heart J*, vol. 31, no. 19, pp. 2369-429, Oct, 2010.

- [4] S. Nattel, "New ideas about atrial fibrillation 50 years on," *Nature*, vol. 415, no. 6868, pp. 219-226, 2002.
- [5] P. Sanders, O. Berenfeld, M. Hocini, P. Jais, R. Vaidyanathan, L. F. Hsu, S. Garrigue, Y. Takahashi, M. Rotter, F. Sacher, C. Scavee, R. Ploutz-Snyder, J. Jalife, and M. Haissaguerre, "Spectral analysis identifies sites of high-frequency activity maintaining atrial fibrillation in humans," *Circulation*, vol. 112, no. 6, pp. 789-97, Aug 9, 2005.
- [6] K. Nademanee, J. McKenzie, E. Kosar, M. Schwab, B. Sunsaneewitayakul, T. Vasavakul, C. Khunnawat, and T. Ngarmukos, "A new approach for catheter ablation of atrial fibrillation: mapping of the electrophysiologic substrate," J Am Coll Cardiol, vol. 43, no. 11, pp. 2044-53, Jun 2, 2004.
- [7] S. M. Narayan, D. E. Krummen, K. Shivkumar, P. Clopton, W. J. Rappel, and J. M. Miller, "Treatment of atrial fibrillation by the ablation of localized sources: CONFIRM (Conventional Ablation for Atrial Fibrillation With or Without Focal Impulse and Rotor Modulation) trial," *J Am Coll Cardiol*, vol. 60, no. 7, pp. 628-36, Aug 14, 2012.
- [8] Y. Huo, T. Gaspar, R. Schönbauer, M. Wójcik, L. Fiedler, F. X. Roithinger, M. Martinek, H. Pürerfellner, B. Kirstein, U. Richter, S. Ulbrich, J. Mayer, O. Krahnefeld, T. Agdirlioglu, A. Zedda, J. Piorkowski, and C. Piorkowski, "Low-voltage myocardium-guided ablation trial of persistent atrial fibrillation," *NEJM Evidence*, vol. 1, no. 11, 2022.
- [9] J. Merino Llorens, S. Kim, M. Martinez Cossiani, J. Relan, M. San Roman, S. Castrejon Castrejon, M. Jauregui Abularach, L. Guido Lopez, D. Merino, and C. Escobar Cervantes, "Systematic identification of low voltage-high frequency electrogram zones at sites of left atrial reentrant tachycardia termination," *Europace*, vol. 25, no. Supplement_1, pp. euad122. 757, 2023.
- [10] I. Sim, M. Bishop, M. O'Neill, and S. E. Williams, "Left atrial voltage mapping: defining and targeting the atrial fibrillation substrate," *J Interv Card Electrophysiol*, vol. 56, no. 3, pp. 213-227, Dec, 2019.
- [11] J. L. Salinet, J. H. Tuan, A. J. Sandilands, P. J. Stafford, F. S. Schlindwein, and G. A. Ng, "Distinctive patterns of dominant frequency trajectory behavior in drug-refractory persistent atrial fibrillation: preliminary characterization of spatiotemporal instability," *J Cardiovasc Electrophysiol*, vol. 25, no. 4, pp. 371-379, Apr, 2014.
- [12] J. L. Salinet, Jr., J. P. Madeiro, P. C. Cortez, P. J. Stafford, G. A. Ng, and F. S. Schlindwein, "Analysis of QRS-T subtraction in unipolar atrial fibrillation electrograms," *Med Biol Eng Comput*, vol. 51, no. 12, pp. 1381-91, Dec, 2013.
- [13] M. Barandas, D. Folgado, L. Fernandes, S. Santos, M. Abreu, P. Bota, H. Liu, T. Schultz, and H. Gamboa, "TSFEL: Time Series Feature Extraction Library," *SoftwareX*, vol. 11, 2020.

Address for correspondence: Noor Qaqos School of Engineering University of Leicester, UK <u>nnq2@leicester.ac.uk</u>